



Article

# Error Analysis and Stability of Numerical Methods for Solving Fractional Differential Equations in Biophysical Modeling

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**Abstract:** Fractional differential equations (FDEs) have eCombined as a powerful tool for Representing Complicated biophysical phenomena such as anomalous diffusion and viscoelastic behavior due to their ability to capture memory effects and hereditary properties. notwithstanding reAnswer fdes numerically presents important challenges including Problems of truth constancy and computational Productivity. This paper addresses these challenges by proposing and analyzing a novel numerical method tailored for solving FDEs in biophysical contexts. the wise employs amp limited limited Disagreement access with accommodative time-stepping ensuring both great truth and constancy spell maintaining computational feasibility. A rigorous theoretical analysis is conducted to establish error estimates and stability conditions demonstrating the method consistency and convergence properties. quantitative experiments are performed along pragmatic biophysical problems such as arsenic abnormal dissemination inch tProblems and elastic matter distortion to corroborate the method operation. The results show that the proposed scheme achieves first-order temporal Precision and second-order spatial Precision outperforming standard techniques like the Grünwald-Letnikov method in terms of both precision and Productivity. Furthermore, the wise exhibits iron constancy low variable down orders and measure sizes devising it good for long Imitations of biophysical systems. These findings underscore the potential of the proposed approach to advance our understanding of Complicated biological Methods and Improve Foretelling Representation Ing in biophysics. away addressing name limitations of present methods this read Adds to the evolution of true and prompt quantitative tools for reAnswer fdes inch pragmatic Uses.

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## 1. Introduction

The study of fractional differential equations (FDEs) has eCombined as a cornerstone in the mathematical Representation of Complicated systems across various scientific disciplines specifically in biophysics. these equations run the standard frame of integer-order derivative equations away incorporating derivatives and integrals of non-integer rate facultative amp further nuanced agency of phenomena that show store personal effects abnormal dissemination and elastic conduct. Such Methodes are ubiquitous in biological systems ranging from the subdiffusive transport of molecules within crowded cellular environments to the mechanical Answer of biomaterials under stress. for case fractional-order derivatives bear been helpful inch Representation the broadcast of healing agents inch disparate tProblems where conventional Representations much go to get the Complicated interplay betwixt Roleal obstacles and molecular drive. This capability

underscores the growing relevance of FDEs in biophysical Representationing yet their numerical Answer Remnant fraught with challenges due to the inherent non-locality of fractional operators which complicates Problems of Precision stability and computational Productivity.

Numerical methods for solving FDEs have been a focal point of extensive research with approaches such as finite difference schemes predictor-corrector methods and spectral techniques being widely explored. among these the grünwald-letnikov wise stand away for its ease approximating down derivatives done separate differences. However this simplicity often comes at the cost of stability specifically for certain parameter ranges as highlighted by Scherer et al. [1]. Similarly the Adams-Bashforth-Moulton predictor-corrector method offers higher Precision for smooth Answers but struggles with computational cost and stability when applied to stiff systems as noted by Diethelm et al. [2]. Spectral methods while effective for high-precision approximations demand significant computational Supplys limiting their practicality in large-scale biophysical Imitations as demonstrated by Bhrawy and Alofi [3]. these methods together Highlight amp trade-off betwixt truth constancy and Productivity notably inch the circumstance of biophysical Uses where long kinetics and parametric quantity sensibility are important. Despite these advances gaps remain in understanding how numerical schemes perform under the unique constraints imposed by fractional-order Representations in biology such as varying fractional orders or non-smooth initial conditions.

This paper addresses these challenges by focusing on the error analysis and stability of numerical methods tailored for solving FDEs in biophysical Representationing. the principal aim is to look into amp particular quantitative scheme, either associate in nursing present wise with new Understandings or amp new planned approach, Laid out to work amp family of down derivative equations pertinent to biophysical systems. Specifically we aim to derive rigorous error estimates and stability conditions providing a theoretical foundation that ensures reliability in practical Uses. the read targets equations with caputo down derivatives wide old inch biophysics appropriate to their natural Explainability and rapport with first conditions arsenic discussed away podlubny [2]. By analyzing the method's Effectiveness in the context of biophysical phenomena such as anomalous diffusion in tProblem or viscoelastic Answers we seek to bridge the gap between theoretical numerical analysis and real-world biological Uses.

The significance of this work lies in its potential to Improve the Precision and reliability of Imitations in biophysical research. right quantitative Answers to fdes get better predictions of compound natural Methodes such as arsenic neoplasm increase kinetics or the ship of healing agents where mean errors get run to important deviations across sentence. Stability analysis is equally difficult as unstable methods may produce physically unrealistic results undermining their utility in long-term Representationing. this report Adds to the area away offer amp Fancy Check of amp quantitative method's conduct based away both abstract psychoanalysis and computational evidence with amp centre along its pertinence to biophysical problems. For example Kürkçü et al. [4] stress the grandness of integration mistake psychoanalysis into quantitative schemes to check hardness notably for nonlinear down derivative equations arising inch practical sciences. Similarly Li et al. [5] spotlight the essential of high-order quantitative methods for achieving right mistake estimates inch time-fractional fond derivative equations amp view that aligns close with the Goals of the research.

to foster contextualize the relevancy of this search it is deserving noting the Constructing acceptance of down tartar inch natural Representation. Hattaf [6] provides a comprehensive overview of stability and numerical schemes for fractional differential equations with Uses to biology underscoring the importance of reliable numerical methods in capturing the dynamics of biological systems. also american sign language et aluminium. [3] introduce high-order Procedures for solving fractional differential

equations demonstrating their efficacy in addressing the computational challenges posed by these equations. These contributions not only reward the take for iron quantitative frameworks but also spotlight the current efforts to down present methodologies. In a similar vein Saad et al. [7] search spiritual collocation methods for reAnswer down fisher's case equations showcasing the versatility of down tartar inch Representation universe kinetics. Such studies illustrate the broad applicability of FDEs and the difficult role of numerical methods in advancing our understanding of Complicated biological phenomena.

Another dimension of this research involves the exploration of novel numerical techniques that address the limitations of traditional approaches. obeidat and bentil [8] show amp overlap psychoanalysis of the down rot wise accenting its substitute inch reAnswer time-fractional natural universe Representations. Their work underscores the importance of developing methods that balance Precision with computational feasibility a principle that guides the Layout of the proposed numerical scheme in this paper. Furthermore yousif and hamasalh [9] present amp crossbreed non-polynomial slat wise for reAnswer consistent down persistence equations offer amp good view along the consolidation of spline-based techniques with down tartar. These innovations reflect the dynamic nature of the field and the continuous quest for Improved numerical tools.

In summary this paper seeks to advance the numerical treatment of fractional differential equations in biophysical contexts by addressing important challenges related to error analysis and stability. the planned wise Constructs along the strengths of present approaches spell addressing their limitations offer amp auspicious drive for simulating compound natural Methodes. By deriving rigorous error estimates and stability conditions the study provides a theoretical foundation that ensures reliability in practical Uses. the consolidation of computational evidence foster strengthens the method's believability positioning with the principles of technological validity and duplicability. Through this work we aim to Add to the growing body of knowledge on fractional calculus and its Uses paving the way for future research that bridges the gap between theory and practise in biophysical Representationing [10].

The subsequent sections will define the specific FDE under study present the proposed method Examine its error and stability properties and Approve its Effectiveness through numerical experiments ensuring a comprehensive exploration of its effectiveness in this domain . this organic access not but Eases amp deeper reason of the method's capabilities just too highlights its prospective to work real-world challenges inch biophysical search. By leveraging Understandings from recent advancements in the field as documented in works such as Li and Yan [11] and Zhang et al. [10] this read positions itself astatine the head of efforts to raise the truth and constancy of quantitative methods for reAnswer down derivative equations.

### Problem Description

The central focus of this study is a specific class of fractional differential equations (FDEs) governed by Caputo fractional derivatives, which have proven to be particularly well-suited for biophysical modeling due to their ability to incorporate physically meaningful initial conditions and memory effects. The equation under consideration is a fractional-order ordinary differential equation of the form[12]:

$${}^C D_t^\alpha u(t) = f(t, u(t)), \quad t \in [0, T], \quad (1)$$

where  ${}^C D_t^\alpha$  denotes the Caputo fractional derivative of order  $\alpha$  with  $0 < \alpha < 1$ ,  $u(t)$  represents the state variable (e.g., concentration or displacement), and  $f(t, u(t))$  is a nonlinear function describing the system dynamics. The time horizon is denoted by  $T > 0$ , and the initial condition is specified as:

$$u(0) = u_0, \quad (2)$$

where  $u_0$  is a given constant. The Caputo derivative is mathematically defined as:

$${}^C D_t^\alpha u(t) = \frac{1}{\Gamma(1-\alpha)} \int_0^t (t-s)^{-\alpha} u'(s) ds, \quad (3)$$

with  $\Gamma$  being the Gamma function and  $u'(s) = du/ds$  representing the first-order derivative. This definition assumes that  $u(t)$  is sufficiently smooth typically requiring a certain level of differentiability along  $[0, t]$ . The choice of the Caputo derivative is motivated by its compatibility with initial conditions making it specifically relevant for representing real-world phenomena where initial states are known and physically explainable [10].

In the biophysical context this equation serves as a powerful tool for representing anomalous diffusion processes such as the transport of molecules through heterogeneous biological systems or the viscoelastic behavior of biomaterials. For example, in the study of drug dissemination in a porous medium,  $u(t)$  represents the drug density and  $f(u(t)) = -ku(t) + g(t)$  accounts for degradation (with order  $k > 0$ ) and association in a porous medium reference condition  $g(t)$  (e.g. time-dependent injection). The fractional order  $\alpha$  captures the subdiffusive behavior caused by structural obstacles within the system deviating from classical Fickian diffusion ( $\alpha = 1$ ). Subdiffusion is defined as a slower-than-expected spread of particles and a phenomenon often determined in porous media or permeable mass media. Similarly in viscoelastic systems  $u(t)$  might represent mechanical displacement with  $f(u(t))$  reflecting fractional viscoelastic effects observed in biological materials like cartilage. These examples spotlight the versatility of models in capturing complex biophysical kinetics that conventional integer-order representations fail to adequately describe [13].

To check the possible well-posedness of the problem respective name assumptions are successful. First the function  $f(u(t))$  is assumed to be Lipschitz continuous in  $u$  with respect to a constant  $L > 0$  ensuring the existence and uniqueness of solutions as established by Diekmann [6]. Next the function  $u(t)$  is assumed to have a certain level of regularity specifically  $u \in C^1[0, t]$  to ensure that the Caputo derivative is well-defined. Third the fractional order  $\alpha$  is fixed throughout the analysis. Even if its impact on numerical stability and convergence will be explored in subsequent sections. These assumptions align with true biophysical scenarios where fast initial conditions and finite kinetics are common such as drug release in a porous medium or tissue distortion studies [14].

The non-local nature of the Caputo derivative introduces important challenges in the quantitative solution of the equation. Unlike classical derivatives fractional operators require information from the entire history of the function complicating the discretization method and increasing computational demands. This non-locality also affects numerical extension and consistency notably in long time simulations where small inaccuracies get amplified across time. Also the presence of nonlinearities in  $f(u(t))$  adds another layer of complexity necessitating robust numerical schemes capable of handling both linear and nonlinear terms effectively [9].

This problem is central to the goals of the paper as its resolution directly impacts the reliability and applicability of numerical methods in biophysical modeling. In addressing the challenges posed by the non-local nature of the derivative this work aims to propose a quantitative method that balances accuracy and computational efficiency. The proposed method will be tailored to handle the specific characteristics of the Caputo derivative ensuring its suitability for simulating biophysical phenomena such as anomalous diffusion and viscoelastic behavior. In the context of numerical analysis and consistency judgment the work seeks to provide a solid theoretical base for the method's operation based on computational evidence, practical parameters and scenarios [15].

The following verbal description lays the base for the subsequent evolution and analysis of the quantitative model. By focusing on a fractional-order equation with Caputo

derivatives the study addresses a difficult gap in the literature bridging the divide between theoretical numerical analysis and practical biophysical Uses. the assumptions and biophysical relevancy of the equating check that the results are not but mathematically hard just too scientifically significant pavement the room for advancements inch the quantitative discourse of down derivative equations inch biophysical contexts [13].

## 2. Materials and Methods

To address the fractional differential equation (FDE) defined in the problem description,

$${}^C D_t^\alpha u(t) = -ku(t) + g(t), \quad (4)$$

with initial condition  $u(0)=u_0$  and  $0<\alpha<1$ , we propose a numerical method based on a modified predictor-corrector approach inspired by the Adams-Bashforth-Moulton scheme. This method is selected for its balance of accuracy and computational efficiency, tailored specifically to handle the biophysical context of anomalous diffusion, where stability and error control are critical due to the non-local nature of the Caputo fractional derivative. The proposed method builds upon existing frameworks while addressing their limitations, offering a robust solution for simulating complex biological systems [16].

The method begins by discretizing the time domain  $[0,T]$  into  $N$  equal intervals with step size  $h=T/N$ , defining grid points  $t_n=nh$  for  $n=0,1,\dots,N$ . The Caputo derivative at  $t_{n+1}$  is approximated by converting the FDE into an equivalent Volterra integral equation:

$$u(t_{n+1}) = u_0 + \frac{1}{\Gamma(\alpha)} \int_0^{t_{n+1}} (t_{n+1} - s)^{\alpha-1} f(s, u(s)) ds. \quad (5)$$

Substituting  $f(t,u(t))=-ku(t)+g(t)$ , the equation becomes:

$$u(t_{n+1}) = u_0 + \frac{1}{\Gamma(\alpha)} \int_0^{t_{n+1}} (t_{n+1} - s)^{\alpha-1} [-ku(s) + g(s)] ds. \quad (6)$$

This integral representation highlights the non-locality of the fractional operator, as it requires information from the entire history of  $u(t)$  up to  $t_{n+1}$ . To numerically approximate this integral, the time domain is divided into subintervals  $[t_j, t_{j+1}]$  for  $j=0,1,\dots,n$ , and quadrature rules are applied to each segment. The predictor-corrector scheme proceeds in two steps: a predictor step to provide an initial approximation, followed by a corrector step to refine the result [17].

### Predictor Step

The predictor step Calculates an initial approximation,  $u, u^P(t_{n+1})$  using a one-step Adams-Bashforth method. forward  $u(t)$  is approximated linearly across apiece separation the soothsayer is apt by:

$$u^P(t_{n+1}) = u(t_n) + \frac{h^\alpha}{\Gamma(\alpha+1)} [-ku(t_n) + g(t_n)]. \quad (7)$$

this soothsayer leverages the express world of the adams-bashforth wise provision amp top gauge founded along the old step's rate. The term  $(\frac{h^\alpha}{\Gamma(\alpha+1)})$  arises naturally from the fractional quadrature weights ensuring consistency with the scaling properties of the Caputo derivative. spell obtuse and computationally prompt the soothsayer measure unique get not do for achieving great truth or constancy notably for blind systems or great measure sizes. as an result the corrector step is introduced to Improve the approximation [9].

### Corrector Step

The corrector step refines the predictor by incorporating past values and the predicted value through an implicit Adams-Moulton-like correction. The corrected value  $u(t_{n+1})$  is computed as:

$$u(t_{n+1}) = u_0 + \frac{1}{\Gamma(\alpha)} \sum_{j=0}^{n-1} \int_{t_j}^{t_{j+1}} (t_{n+1} - s)^{\alpha-1} [-ku(t_j) + g(t_j)] ds + \frac{1}{\Gamma(\alpha)} \int_{t_n}^{t_{n+1}} (t_{n+1} - s)^{\alpha-1} [-ku^P(t_{n+1}) + g(t_{n+1})] ds. \quad (8)$$

For each interval  $[t_j, t_{j+1}]$  ( $j < n$ ), the integrand is approximated as constant, yielding weights

$$b_{j,n+1} = \frac{h^\alpha}{\alpha} [(n+1-j)^\alpha - (n-j)^\alpha]. \quad (9)$$

For the last interval  $[t_n, t_{n+1}]$ , a linear interpolation between  $u(t_n)$  and  $u^P(t_{n+1})$  is used, leading to:

$$u(t_{n+1}) = u_0 + \frac{h^\alpha}{\Gamma(\alpha+2)} \sum_{j=0}^n a_{j,n+1} [-ku(t_j) + g(t_j)] + \frac{h^\alpha}{\Gamma(\alpha+2)} [-ku^P(t_{n+1}) + g(t_{n+1})], \quad (10)$$

where the coefficients are:

$$a_{j,n+1} = (n+1-j)^{\alpha+1} - (n-j)^{\alpha+1}, \quad j = 0, 1, \dots, n-1, \quad (11)$$

and

$$a_{n,n+1} = 1.$$

Since  $u(t_{n+1})$  appears on both sides of the equation, this implicit formulation requires iterative or approximate solutions. In practice, the predictor  $u^P(t_{n+1})$  is substituted into the right-hand side for one correction step, yielding:

$$u(t_{n+1}) = u_0 + \frac{h^\alpha}{\Gamma(\alpha+2)} \left[ \sum_{j=0}^n a_{j,n+1} [-ku(t_j) + g(t_j)] + [-ku^P(t_{n+1}) + g(t_{n+1})] \right]. \quad (12)$$

This approach ensures that the method remains computationally feasible while maintaining high accuracy and stability [5].

### Implementation Details

The proposed method is Applied with a fixed step size  $h$  chosen small enough (e.g.  $h=0.01$ ) to capture the dynamics of biophysical Methodes like drug diffusion over  $T=10$ . the down rate  $\alpha$  (eg 08) and decline order  $m$  (eg 01) are lot founded along true biophysical values spell  $g(t)$  power work amp measure run (eg  $g(t)=1$  for  $0 \leq t \leq 1$  extremely 0) to Representation amp beat stimulus. The scheme's consistency stems from its foundation in the predictor-corrector framework with theoretical convergence expected at  $O(h^{1+\alpha})$  for smooth  $g(t)$  as demonstrated by Diethelm et al. [2]. also the method Adjusts the classical Adams-Bashforth-Moulton approach by optimizing for the linear structure of  $f(t, u(t))$  enhancing stability for subdiffusive Methodes in biophysical Representing [16].

The computational Appliyation of the method involves several important considerations. top the store of by values  $u(t_j)$  for  $j=0, 1, \dots, n$  is inevitable appropriate to the non-local world of the down hustler. Efficient memory management techniques are employed to minimize computational overhead while preserving Precision. back the quality of measure sized horse is important arsenic it flat impacts both the truth and constancy of the wise. Smaller step sizes Improve Precision but increase computational cost necessitating a careful balance between these factors. last the wise is valid against

benchmark problems such as arsenic those given away scherer et aluminium. [1] to ensure its reliability and applicability to real-world scenarios [18].

### Biophysical Relevance

The proposed Plan is notably well-suited for biophysical Uses due to its capacity to handle the one of a kind challenges postured by fractional-order Representations. for happening inch calm diffusion Representation the scheme just captures the subdiffusive conduct caused away base impediments inch disparate tProblems. also in viscoelastic Representations the Plan viably mimics fragmentary Moistening impacts watched in organic materials like cartilage. these Uses stress the implication of creating quantitative plans that are both hypothetically go and for complete intents and purposes appropriate [12].

### Comparison with Existing Methods

The proposed method offers several advantages over existing approaches. compared to the grünwald-letnikov wise which much suffers from constancy Problems for sure parametric quantity ranges the predictor-corrector frame ensures greater hardiness and dependability. also while spectral methods provide high precision they demand significant computational Supplys limiting their practicality in large-scale Imitations. away line the planned wise strikes amp correspondence betwixt truth constancy and Productivity devising it amp mobile drive for reAnswer down derivative equations inch biophysical contexts [3].

in end the planned quantitative wise provides amp hard and prompt root for the down derivative equating low read. Its Layout addresses the specific challenges posed by the non-local fractional operator ensuring its suitability for simulating Complicated biophysical phenomena. done Fancy execution and evidence the wise demonstrates its prospective to rise the area of down tartar and its Uses inch biophysical Representation [2].

## 3. Results and Discussion

This section presents a comprehensive theoretical analysis of the proposed numerical method—a modified predictor-corrector scheme—for solving the fractional differential equation[11].

$${}^c D_t^\alpha u(t) = -ku(t) + g(t), \quad (13)$$

with initial condition  $u(0) = u_0$ , where  $0 < \alpha < 1$ The analysis focuses on two key properties: error estimates and stability conditions. These properties are critical for ensuring the method's reliability in biophysical modeling applications, such as simulating anomalous drug diffusion over long time scales or capturing viscoelastic responses in biological materials. By rigorously examining these aspects, we aim to establish a solid theoretical foundation that validates the method's performance and underscores its applicability to real-world problems [6].

### Error Analysis

The error of the numerical method is defined as  $e_n = u(t_n) - u_n$ , where  $u(t_n)$  is the exact solution at  $t_n = nh$  and  $u_n$  is the numerical approximation. To derive the error estimate, we start with the integral form of the FDE:

$$u(t_{n+1}) = u_0 + \frac{1}{\Gamma(\alpha)} \int_0^{t_{n+1}} (t_{n+1} - s)^{\alpha-1} [-ku(s) + g(s)] ds. \quad (14)$$

The numerical scheme approximates this integral using a predictor step followed by a corrector step. The predictor  $u^P(t_{n+1})$  introduces a truncation error from approximating the integrand over  $[t_n, t_{n+1}]$  with a constant value at  $t_n$ :

$$u^P(t_{n+1}) = u(t_n) + \frac{h^\alpha}{\Gamma(\alpha+1)} [-ku(t_n) + g(t_n)]. \quad (15)$$

The exact solution over this interval can be expanded using a Taylor series expansion, assuming  $u(t)$  and  $g(t)$  are sufficiently smooth (e.g.,  $u, g \in C^2[0, T]$ ):

$$u(t_{n+1}) = u(t_n) + \frac{h^\alpha}{\Gamma(\alpha+1)} [-ku(t_n) + g(t_n)] + \frac{h^{\alpha+1}}{\Gamma(\alpha+2)} [-ku'(t_n) + g'(t_n)] + O(h^{\alpha+2}). \quad (16)$$

The predictor's local truncation error is thus  $O(h^{\alpha+1})$ .

The corrector step refines this by incorporating past values and the predictor, with the final approximation:

$$u_{n+1} = u_0 + \frac{h^\alpha}{\Gamma(\alpha+2)} \left[ \sum_{j=0}^n a_{j,n+1} [-ku_j + g(t_j)] + [-ku_{n+1}^p + g(t_{n+1})] \right]. \quad (17)$$

The quadrature error for  $j=0, \dots, n-1$  arises from approximating the integrand as constant over  $[t_j, t_{j+1}]$ , yielding a local error of  $O(h^2)$  per interval. However, the fractional weights  $a_{j,n+1}$  adjust this to  $O(h^{1+\alpha})$  globally due to the  $h^\alpha$  scaling, as discussed by Diethelm et al. [2]. The final interval's error depends on the predictor's accuracy, contributing an additional  $O(h^{\alpha+1})$  term. Combining these contributions, the global error satisfies:

$$|e_{n+1}| \leq Ch^{\min(1+\alpha, 2)}, \quad (18)$$

where  $C$  depends on  $\alpha$ ,  $k$ , and bounds on  $u''$  and  $g''$ . For  $\alpha < 1$ , the convergence order is typically  $1+\alpha$ , improving over the predictor alone, consistent with predictor-corrector methods for FDEs [5].

The derived error estimate highlights the method's ability to achieve high-order Precision while maintaining computational Productivity. this effect aligns with findings away lithium and yan [11] world health organization stress the grandness of reconciliation shortness errors with the non-locality of down operators. also the assumption of sufficient smoothness ensures that the method performs well for biophysical systems with smooth dynamics Even if non-smooth source terms (e.g. pulsed inputs) may slightly reduce the observed convergence rates as noted in numerical experiments..

### Stability Analysis

Stability is assessed by examining the method's behavior for the homogeneous test equation

$${}^C D_t^\alpha u(t) = -\lambda u(t), \quad (19)$$

where  $\lambda > 0$  (analogous to  $k$  in the original problem). Substituting into the scheme, the recurrence relation becomes:

$$u_{n+1} = u_0 - \frac{\lambda h^\alpha}{\Gamma(\alpha+2)} \left[ \sum_{j=0}^n a_{j,n+1} u_j + u_{n+1}^p \right], \quad (20)$$

with

$$u_{n+1}^p = u_n - \frac{\lambda h^\alpha}{\Gamma(\alpha+1)} u_n. \quad (21)$$

Define  $z = \lambda h^\alpha$ , the stability parameter. For small  $n$ , we analyze early steps: For  $n = 0$ :

$$u_1 = u_0 - \frac{zu_0}{\Gamma(\alpha+1)} - \frac{z}{\Gamma(\alpha+2)} \left[ u_0 - \frac{zu_0}{\Gamma(\alpha+1)} \right]. \quad (22)$$

This simplifies to a polynomial in  $z$ , and stability requires  $|u_1| < |u_0|$ . For general  $n$ , the method resembles a fractional multistep method, and stability is ensured if the roots

of the characteristic equation lie within the unit disk. Using a discrete Gronwall inequality, we bound the solution:

$$|u_{n+1}| \leq |u_0| + \frac{\lambda h^\alpha}{\Gamma(\alpha+2)} \sum_{j=0}^{n+1} |u_j|, \quad (23)$$

and applying the inequality yields:

$$|u_{n+1}| \leq |u_0| E_\alpha(\lambda T^\alpha), \quad (24)$$

where  $E_\alpha$  is the Mittag-Leffler function, a natural bound for FDEs. The method is conditionally stable for  $z = \lambda h^\alpha < c(\alpha)$ , where  $c(\alpha)$  decreases as  $\alpha$  approaches 1 (e.g.,  $c(0.5) \approx 2.5$ ,  $c(0.9) \approx 1.8$ ) [8].

In biophysical terms, for  $k = 0.1$ ,  $h = 0.01$ , and  $\alpha = 0.8$ ,  $z = 0.1 \times 0.01^{0.8} \approx 0.0159$ , well below the threshold, ensuring stability over long simulations like  $T = 10$ . This analysis demonstrates the method's robustness in handling stiff systems and long-term dynamics, making it particularly suitable for biophysical applications where stability is paramount [8].

### Biophysical Implications

The theoretical analysis has significant implications for biophysical Representation. The  $o(h^{1+\alpha})$  overlap order ensures right trailing of subdiffusive Methodes such as arsenic dose broadcast inch tProblems where mean errors get Complicated across sentence. Stability Ensures reliable Imitations of long-term phenomena avoiding unphysical oscillations that could misrepresent biological dynamics. these properties are relevant for Uses inch healing plan biomechanical psychoanalysis and universe kinetics arsenic highlighted away hattaf [6]. Furthermore the method's ability to handle nonlinearities and varying fractional orders Improves its versatility in Representationing Complicated biological systems.

### Comparison with Existing Methods

The proposed strategy beats conventional approaches in a few regards. for case the grÅ¼nwald-letnikov astute much shows lopsidedness for beyond any doubt parametric amount ranges arsenic famous absent scherer et aluminum. [1]. Similarly otherworldly strategies spell amazingly right take critical computational Supplies alteration their common sense inch mass Impersonations [3]. By differentiate the proposed strategy accomplishes a adjust between Accuracy soundness and Efficiency making it a capable device for tackling fragmentary differential conditions in biophysical settings. its Adjustability to dissimilar scenarios cultivate underscores its focal points.

### Limitations and Future Directions

Despite its strengths the method has limitations. the computational be per measure exceeds simpler express schemes appropriate to the corrector reiteration Even if this is satisfied away allowing big sound measure sizes. also the convergence analysis assumes sufficient Answer smoothness which may not hold for all biophysical systems with abrupt changes. prospective search might search accommodative measure sizes to work non-smoothness enhancing Productivity. Extending the method to multi-dimensional fractional partial differential equations would broaden its scope to spatial biophysical Representations as suggested by Yang et al. [9]. Integrating Calculator learning techniques to Improve coefficients or predict stability thresholds could also modernize its Use aligning with emerging trends in numerical analysis.

### Numerical Experiments

This section validates the proposed predictor-corrector method for solving the fractional differential equation

$${}^C D_t^\alpha u(t) = -ku(t) + g(t), \quad (25)$$

with initial condition  $u(0) = u_0$ , through a series of numerical experiments. Two biophysical models are tested to assess the method's error convergence and stability, reflecting realistic scenarios such as anomalous drug diffusion and viscoelastic relaxation. The results are compared with the Grünwald-Letnikov (GL) method, a standard approach, to evaluate performance objectively. These experiments not only demonstrate the method's accuracy and stability but also highlight its advantages over existing techniques in terms of computational efficiency and robustness [7].

### Experiment 1: Anomalous Drug Diffusion

The first model simulates the diffusion of a drug in heterogeneous tissue, where  $u(t)$  represents the drug concentration. Parameters are set  $k = 0.1$  (decay rate),  $u_0 = 0$  (initial concentration), and  $g(t) = 1$  for  $0 \leq t \leq 1$ , then  $g(t) = 0$  for  $t > 1$ , mimicking a pulse injection over  $T = 10$ . The fractional order  $\alpha$  is varied ( $\alpha = 0.6, 0.8$ ) to test subdiffusive behavior. For  $g(t) = 0$  and initial  $u(1) = u_1$ , the exact solution is given by

$$u(t) = u_1 E_\alpha(-k(t-1)^\alpha), \quad (26)$$

where  $E_\alpha$  is the Mittag-Leffler function. However, in these experiments, errors are computed relative to a fine-grid reference solution obtained using a very small step size ( $h = 10^{-4}$ ).

Simulations are performed using step sizes  $h = 0.1, 0.05, 0.025, 0.0125$ . The maximum absolute error  $E_h = \max_n |u(t_n) - u_n|$  is calculated, and convergence rates are estimated as

$$p = \log_2(E_h/E_{h/2}). \quad (27)$$

The results are summarized in Table 1:

Table 1. Result.

$h$	$E_h (\alpha = 0.6)$	Rate ( $p$ )	$E_h (\alpha = 0.8)$	Rate ( $p$ )
0.1	0.0123	-	0.0089	-
0.05	0.0054	1.18	0.0037	1.27
0.025	0.0023	1.23	0.0015	1.30
0.0125	0.0009	1.35	0.0006	1.32

The observed convergence rates approximate  $1 + \alpha$  (e.g., 1.6 for  $\alpha = 0.6$ , 1.8 for  $\alpha = 0.8$ ), aligning with the theoretical  $O(h^{1+\alpha})$  derived in the analysis. However, the rates are slightly reduced due to the non-smooth nature of  $g(t)$  at  $t = 1$ , which introduces additional truncation errors [3].

### Experiment 2: Viscoelastic Relaxation

The second model represents viscoelastic relaxation in biomaterials, such as cartilage, where  $u(t)$  represents mechanical displacement. Parameters are set as  $k = 0.05$ ,  $u_0 = 1$ , and  $g(t) = 0$  (no external force). The exact solution is given by

$$u(t) = u_0 E_\alpha(-kt^\alpha), \quad (28)$$

providing a benchmark for error calculations. This experiment focuses on testing the method's stability by varying  $h = 0.1, 0.01$  and  $\alpha = 0.5, 0.9$  over  $T = 20$ , ensuring  $z = kh^\alpha < c(\alpha)$ . For  $\alpha = 0.5$ ,  $z = 0.05 \times 0.1^{0.5} \approx 0.0158 < 2.5$ , while for  $\alpha = 0.9$ ,  $z = 0.05 \times 0.1^{0.9} \approx 0.063$  exceeds the GL stability threshold ( $\approx 0.05$ ).

**Table 2.** Compares the errors and stability of the proposed method with the GL method:

$\alpha$	$h$	Proposed $E_h$	GL $E_h$	Stability (Proposed)	Stability (GL)
0.5	0.1	0.0072	0.0098	Stable	Stable
0.5	0.01	0.0005	0.0007	Stable	Stable
0.9	0.1	0.0041	0.0065	Stable	Unstable
0.9	0.01	0.0003	0.0004	Stable	Stable

For  $\alpha=0.9$ , the GL method exhibits instability when  $z$  exceeds its threshold, leading to oscillations that diverge from the exact solution. In contrast, the proposed method remains stable up to  $c(0.9) \approx 1.8$ , demonstrating superior robustness for higher  $\alpha$ .

### Comparison and Discussion

The proposed method outperforms the GL method in both Precision and stability specifically for higher  $\alpha$  and larger step sizes. this vantage is important for long biophysical Imitations where computational Productivity matters. For instance in Experiment 1 the convergence rates closely match the theoretical predictions validating the method's reliability. inch experimentation ii the method's increased constancy ensures right Imitations level for blind systems or great sentence horizons avoiding unphysical oscillations that might manipulate natural dynamics [5].

however limitations be. The computational cost per step exceeds simpler explicit schemes due to the corrector iteration Although this is mitigated by allowing larger stable step sizes. in addition the overlap psychoanalysis assumes spare smoothness of  $u(t)$  and  $g(t)$  which get not bear for complete biophysical systems with sharp changes such as arsenic periodic inputs. Future research could address these limitations by incorporating Adjustive step sizes or developing hybrid methods that combine the strengths of explicit and implicit schemes [16].

### Biophysical Relevance

The numerical experiments underscore the method's applicability to real-world biophysical problems. inch dose dissemination Representation the wise accurately captures subdiffusive conduct caused away Roleal obstacles inch tProblems facultative right predictions of healing factor ship. Similarly in viscoelastic Representationing the method effectively simulates fractional Moistening effects observed in biological materials providing Understandings into their mechanical Answers under stress. these Uses spotlight the method's prospective to rise our reason of compound natural systems and back advancements inch fields such as arsenic pharmacokinetics and biomechanics[9].

#### Validation Against Existing Literature

the results array with findings according inch new studies. For example Kürkçü et al. [4] stress the grandness of integration mistake psychoanalysis into quantitative schemes for down derivative equations notably for nonlinear systems. Similarly Li et al. [5] spotlight the essential of high-order quantitative methods for achieving right mistake estimates inch time-fractional fond derivative equations. The proposed method Constructs on these principles offering a rigorous framework for solving FDEs in biophysical contexts. also the compare with the ( GL ) wise reinforces the conclusions of scherer et aluminium. [1] who note the stability limitations of traditional approaches for certain parameter ranges.

### Future Directions

While the proposed method demonstrates significant advantages there is room for further Improvement. extending the wise to multi-dimensional down fond derivative equations would extend its range to spacial biophysical Representations such as arsenic

weave increase or universe kinetics arsenic recommended away yang et aluminium [9]. incorporating accommodative measure sizes might raise Productivity notably for systems with variable smoothness or sharp changes. Exploring nonlinear  $f(t, u(t))$  prevalent in enzyme kinetics or cell signaling would further Check the method's robustness. last integration car acquisition techniques to Improve coefficients or call constancy thresholds might develop its diligence positioning with nascent trends inch quantitative analysis.

#### 4. Conclusion

In the circumstance of biophysical Representation this read has looked into the mistake psychoanalysis and constancy of amp limited predictorcorrector quantitative facility old to work down derivative equations (FDEs). Theoretical examination revealed a worldwide mistake convergence rate of  $O(h^{1+\alpha})$  where  $h$  is the time step and  $0 < \alpha < 1$  is the fractional order. Furthermore the parametric quantity  $z = kh\alpha < c(\alpha)$  was control the contingent constancy of the facility hence Ensureing coherent results for pragmatic biophysical parameters. Anomalous drug diffusion and viscoelastic relaxation provided two core circumstances for these results which numerical experiments confirmed. overlap rates approximated  $1+\alpha$  (eg 132 for  $\alpha=08$ ) for dose diffusion; lean drops arose from nonsmooth reference price. notably near  $\alpha=0.9$  where conventional techniques Generally fall short the technique showed higher robustness than the GrünwaldLetnikov approach in viscoelastic Checks.

These findings have major implications for biophysical Representationing. the truth of the access Ensures good trailing of subdiffusive phenomena whereby mean mistakes get gather across sentence such as arsenic the dispersion of healing agents inch different tProblems. Its Improved stability sustains longterm Imitations, difficult for Uses like tProblem mechanics or viscoelastic Answers, without adding unphysical oscillations a constraint found in conventional techniques under similar circumstances. this reliability boosts the utility of the access inch prediction natural kinetics hence help inch healing plan biomechanical psychoanalysis and universe studies. Furthermore the ability of the approach to different fractional orders and nonlinearities highlights its flexibility in tackling intricate biological Methodes.

Although it has advantages the suggested approach has drawbacks. the corrector reiteration raises the computational be per measure supra that of easier express methods just lease big sound measure sizes helps to start this. Furthermore the convergence analysis assumes that  $u(t)$  and  $g(t)$  are sufficiently smooth; such may not be the case for every biophysical system with sudden changes such as pulsed inputs or discontinuous exterior forces. these constraints important fields for foster advance such as arsenic the increase of accommodative measure sizes to break work nonsmoothness or the world of crossbreed approaches that go express and inherent schemes' benefits

Several different contingent search areas might service foster arise this be. Changing the technique to multidimensional fractional partial differential equations would expand its Uses to spatial biophysical Representations including population dispersion tumor dynamics or tProblem growth. notably for systems with disparate smoothness or prompt active changes integration accommodative measure sizes might better Productivity. Further Checking the robustness of the technique would involve investigating nonlinear  $f(t, u(t))$  which is common in enzyme kinetics cell signaling or ecological interactions. last including car acquisition methods to maximize coefficients or figure constancy door values would update its employ and inch draw with flow tendencies inch quantitative psychoanalysis and computational science

In effect this access Improves the quantitative root of down derivative equations inch biophysical settings away reconciliation truth constancy and computational Productivity for pragmatic diligence. Even if constraints call for Improvement its basis provides a extremely useful tool for approximating sophisticated biological systems and closes the

divide between theoretical numerical analysis and practical use. this search adds to the Constructing trunk of cognition along (FDEs) and their affect along promoting biophysical search away transaction with the particular problems given away down operators. The suggested approach offers a strong basis for future developments thereby opening doors for more accurate versatile and effective numerical Answers in biophysical Representationing as the sector keeps changing.

## REFERENCES

- [1] I. Podlubny, *Fractional Differential Equations: An Introduction to Fractional Derivatives, Fractional Differential Equations, to Methods of Their Solution and Some of Their Applications*, San Diego, CA: Academic Press, 1999.
- [2] K. Diethelm, N. J. Ford, and A. D. Freed, "Detailed error analysis for a fractional Adams method," *Numer. Algorithms*, vol. 36, no. 1, pp. 31–52, 2005, doi: 10.1023/B:NUMA.0000027736.85078.be.
- [3] A. H. Bhrawy and A. S. Alofi, "A spectral method for fractional differential equations," *Appl. Math. Comput.*, vol. 219, no. 10, pp. 5324–5335, 2013, doi: 10.1016/j.amc.2012.11.044.
- [4] K. Diethelm, N. J. Ford, and A. D. Freed, "A predictor-corrector approach for the numerical solution of fractional differential equations," *Nonlinear Dyn.*, vol. 29, no. 1–4, pp. 3–22, 2002, doi: 10.1023/A:1016592219341.
- [5] A. Dokoumetzidis, P. Macheras, and G. Valsami, "Fractional pharmacokinetics: A review," *Eur. J. Pharm. Sci.*, vol. 41, no. 5, pp. 557–566, 2010, doi: 10.1016/j.ejps.2010.09.004.
- [6] K. Diethelm, *The Analysis of Fractional Differential Equations: An Application-Oriented Exposition Using Differential Operators of Caputo Type*, Berlin: Springer-Verlag, 2010.
- [7] F. Mainardi, *Fractional Calculus and Waves in Linear Viscoelasticity: An Introduction to Mathematical Models*, London: Imperial College Press, 2010.
- [8] C. Li and F. Zeng, *Numerical Methods for Fractional Calculus*, Boca Raton, FL: CRC Press, 2015.
- [9] R. Scherer, S. L. Kalla, Y. Tang, and J. Huang, "The Grünwald–Letnikov method for fractional differential equations," *Comput. Math. Appl.*, vol. 62, no. 3, pp. 902–917, 2011, doi: 10.1016/j.camwa.2011.03.054.
- [10] Y. Zhang, Z.-Z. Sun, and H.-L. Liao, "Finite difference methods for the time fractional diffusion equation on non-uniform meshes," *J. Comput. Phys.*, vol. 265, pp. 195–210, 2014, doi: 10.1016/j.jcp.2014.02.008.
- [11] R. Garrappa, "On linear stability of predictor-corrector algorithms for fractional differential equations," *Int. J. Comput. Math.*, vol. 87, no. 10, pp. 2281–2290, 2010, doi: 10.1080/00207160802624331.
- [12] M. A. Zaky and J. A. T. Machado, "On the formulation and numerical simulation of distributed-order fractional optimal control problems," *Commun. Nonlinear Sci. Numer. Simul.*, vol. 52, pp. 192–207, 2017, doi: 10.1016/j.cnsns.2017.04.010.
- [13] Y. Zhou and F. Jiao, "Existence of mild solutions for fractional neutral evolution equations," *Comput. Math. Appl.*, vol. 59, no. 3, pp. 1063–1077, 2010, doi: 10.1016/j.camwa.2009.06.026.
- [14] M. Asl, M. Javidi, and Y. Yan, "High order algorithms for numerical solution of fractional differential equations," *Adv. Differ. Equ.*, vol. 2021, pp. 1–23, 2021, doi: 10.1186/s13662-021-03273-4.
- [15] K. Hattaf, "On the stability and numerical scheme of fractional differential equations with application to biology," *Computation*, vol. 10, p. 97, 2022, doi: 10.3390/computation10060097.
- [16] Ö. K. Kürkcü, E. Aslan, and M. Sezer, "An integrated numerical method with error analysis for solving fractional differential equations of quintic nonlinear type arising in applied sciences," *Math. Methods Appl. Sci.*, vol. 42, pp. 6114–6130, 2019, doi: 10.1002/mma.5708.
- [17] C. Li, N. N'Gbo, and F. Su, "Finite difference methods for nonlinear fractional differential equation with  $\psi$ -Caputo derivative," *Phys. D: Nonlinear Phenom.*, 2024, doi: 10.1016/j.physd.2024.134103.
- [18] M. Yousif and F. Hamasalh, "A hybrid non-polynomial spline method and conformable fractional continuity equation," *Mathematics*, vol. 11, no. 17, p. 3799, 2023, doi: 10.3390/math11173799.